



MEG with the SIS-MEG system
Biophysics Group, Los Alamos National Laboratory



Magnetoencephalography (MEG) in the Biophysics Group

Presented to
The Physics Division Review Committee
(5-6 February 2001)

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Outline

☞ **Background & Introduction**

The Superconducting Imaging Surface (SIS) MEG system
in context to brain imaging & other MEG systems.

☞ **The SIS-MEG system**

Status of the SIS-MEG system
Recent results obtained with the LANL SIS MEG System

☞ **Summary & Future Plans**

Summary of status & results
Future directions & opportunities for SIS-MEG

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Our Collaborators

Albuquerque Veterans Administration Hospital
 MIND Institute
 Sandia National Laboratory
 University of Minnesota / VAMC Minneapolis
 University of New Mexico
 NIS-Division – J. Mosher

Funding

NIH/NINDS; DOE/OBER
 MIND Institute; LANL LDRD

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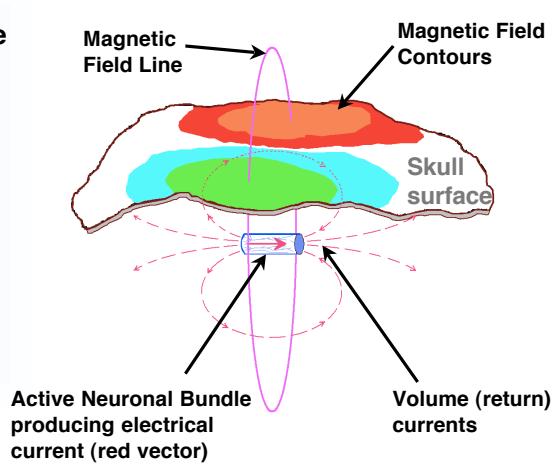
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Background & Introduction

Goal: Noninvasively measure Brain function with high temporal resolution and sufficient spatial definition & signal-to-noise to enable the most accurate source localization.

Address instrumentation issues: Cost, Robustness, Shielding, State-of-art technologies, Precision & Accuracy.



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The SIS System - Motivation (& history)

Novel Basic Imaging concept (*Flynn et al.*)
Image neuronal currents on superconducting surface

Inherent Shielding & Imaging properties
Meissner effect of SIS eliminates most external fields (□ independent)

Improved Performance at Lower Cost
Lower noise, simple SQUID sensor design, materials, fabrication methods.

Incorporate state-of-art Technologies
Control system & real-time analysis tools (MEGAN, Brainstorm)
State-of-art SQUID electronics & sampling technology

→ Prohibitively expensive for industry

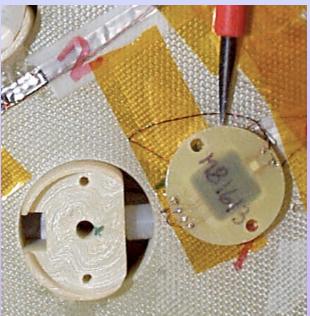
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SQUIDs are the Most Sensitive Magnetic Field Sensors Known

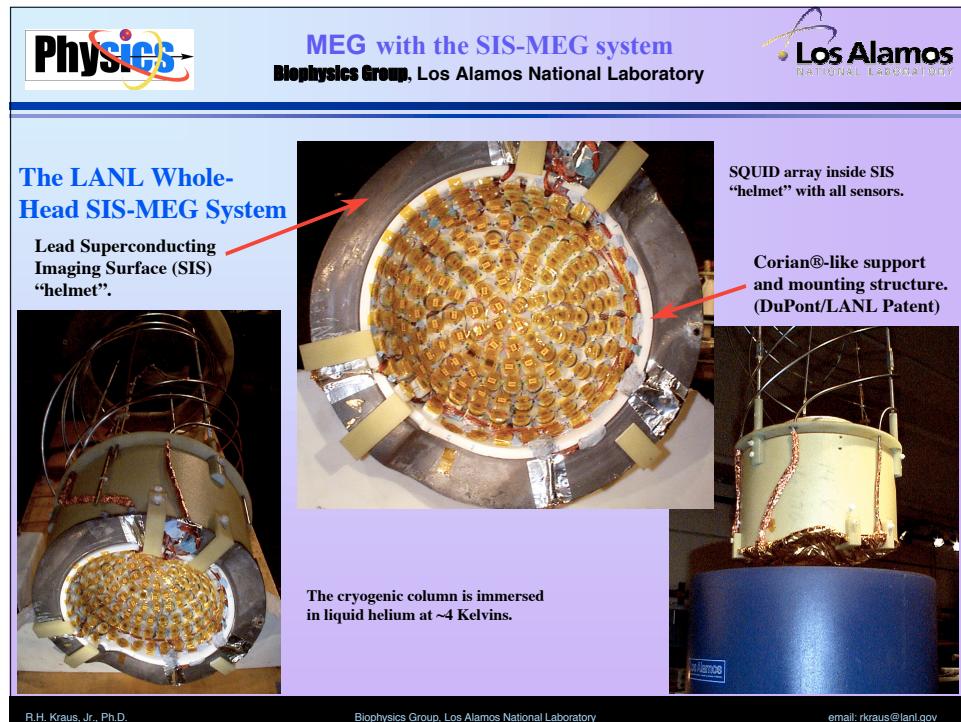


Magnetic Field Scale

Gauss	Tesla
1	10^{-4}
0.1	10^{-5}
10^{-2}	10^{-6}
10^{-3}	10^{-7}
10^{-4}	10^{-8}
10^{-5}	10^{-9}
10^{-6}	10^{-10}
10^{-7}	10^{-11}
10^{-8}	10^{-12}
10^{-9}	10^{-13}
10^{-10}	10^{-14}
10^{-11}	10^{-15}

Earth Magnetic Field (DC Component)
Urban Noise
Magnetic Impurities in the Lungs
Human Heart (QRS Complex)
Skeletal Muscles
Fetal Heart (QRS Complex)
Epileptic Spike
Human Brain (A Rhythm)
HIS Bundle Evoked Response in Brain
Low-T_c SQUID Noise

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Goal of Magnetic Measurements

Study Neuronal Activity:
temporal evolution, spatial localization & evolution

Requirements:

- Maximal S/N*
- Precision/Accuracy of sensor array & sensors ...*
- (assumed but rarely discussed)*
- Complete & accurate description of the forward physics*

Magnetic field distribution measured outside the head

↓ ↓ ↓ ↓

Estimation of source location and temporal evolution

One of the greatest challenges for the SIS-MEG system was describing the forward physics ...

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Analytic Approaches to Describing SIS-MEG Forward physics

Current-loop dipole M_{source} located at $\mathbf{r}=(x_0, y_0, z_0)$, and M_{img} located at $\mathbf{r}'=(x_0, y_0, -z_0)$.

$$\mathbf{B}(\mathbf{r}) = \frac{\mu_0}{4\pi} \left[\frac{\mathbf{M} \cdot \mathbf{R}}{R^3} \mathbf{R} + \frac{3}{(R')^3} \frac{\mathbf{M} \cdot \mathbf{R}'}{R'^3} \mathbf{R}' + \frac{\mathbf{M}}{(R')^3} \right] \quad \text{Planar Imaging-Surface}$$

Current dipole $\mathbf{Q}_{\text{source}}$ located at \mathbf{r}_0 , and \mathbf{Q}_{img} located at $\mathbf{r}=(a/r_0)^2 \mathbf{r}_0$

$$\mathbf{r} \cdot \mathbf{B} = \frac{\mu_0}{4\pi} \frac{1}{R^3} \left[\frac{1}{r^3} - \frac{3}{(R')^3} \right] \quad \text{Spherical Imaging-Surface}$$

But not feasible for complex geometries

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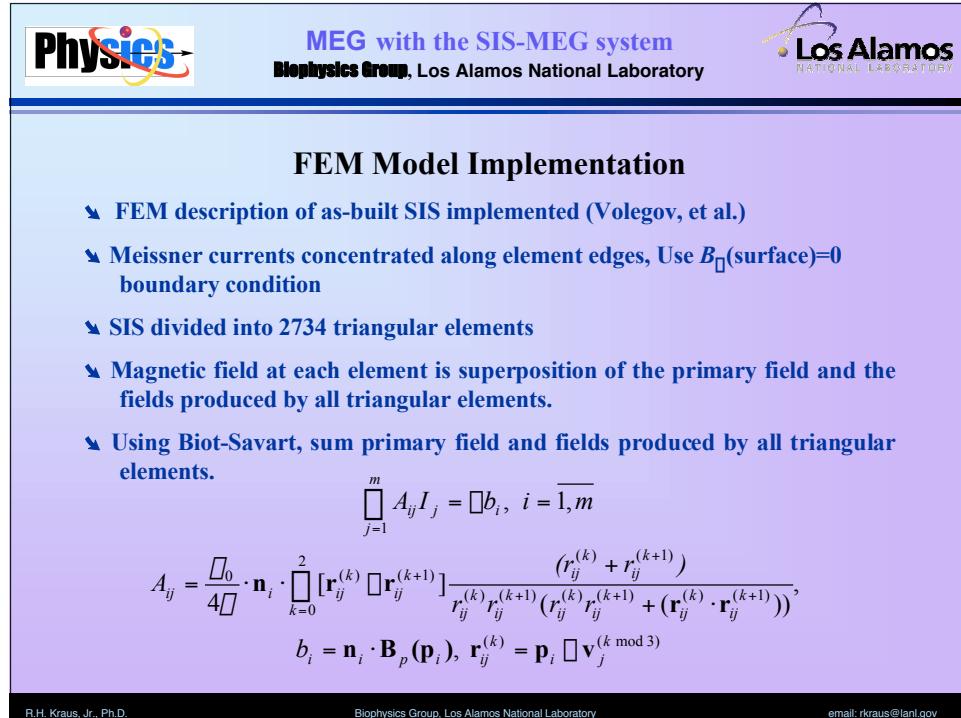
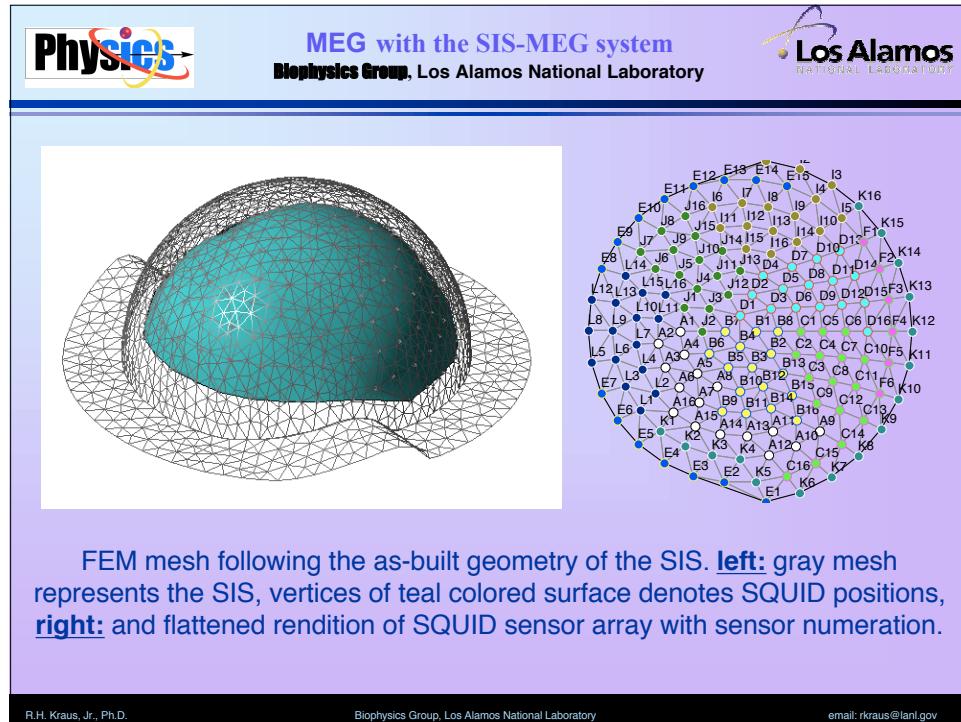
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Effect of Complex shape of SIS Helmet:

Hemispherical helmet with ear cut-outs and brim.

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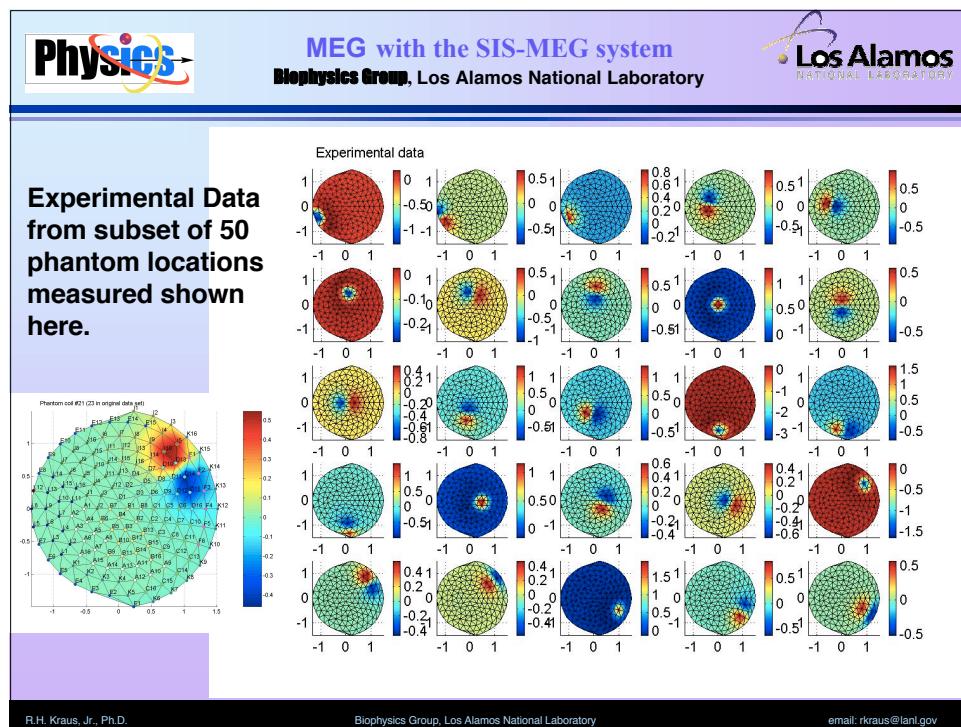


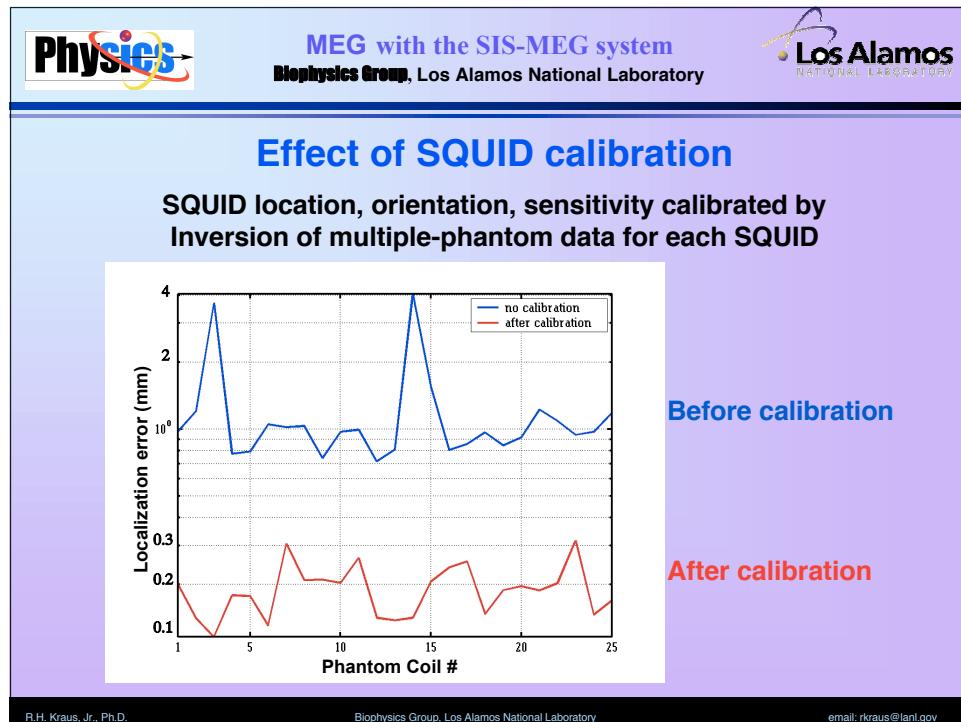
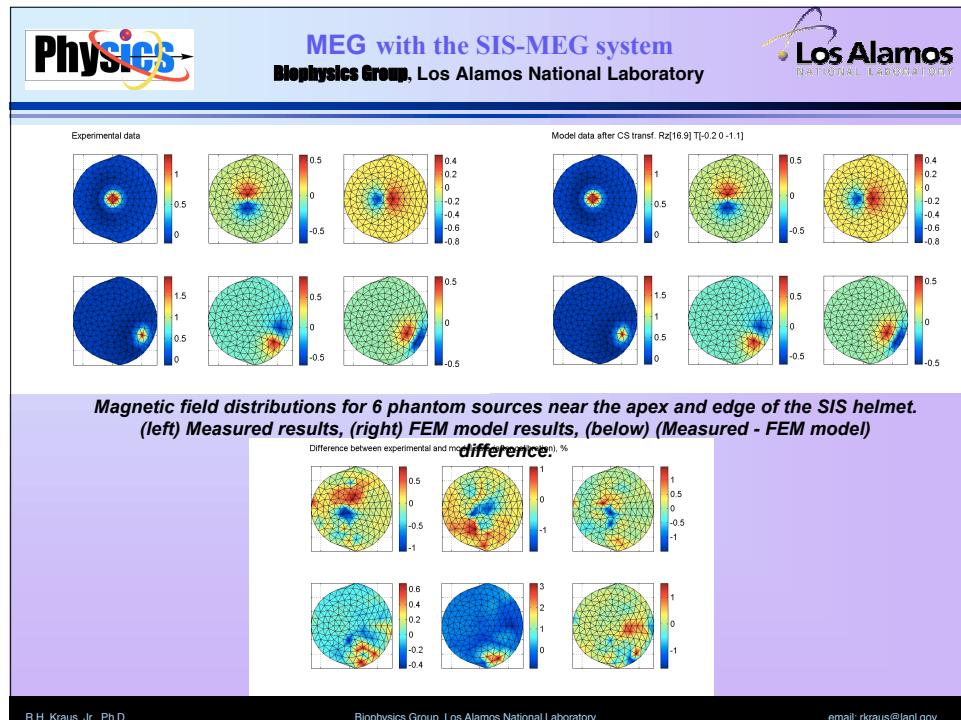
Precision phantoms with well defined source model used to test the SIS-MEG system & description of Forward Physics

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50-coil set Independent Phantom Localization

<Precision> = <0.25mm for all phantom coils.

- previous best reported in literature ~1.5mm

Phantom coil #16 mislocated (during inspection process)

S/N ~20 for equivalent of 770 epochs. Maximal signal nominal 100-500fT.

Multi-dipole, orthogonal time series data. Using calibrated SQUID positions, sensitivities

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Background Shielding

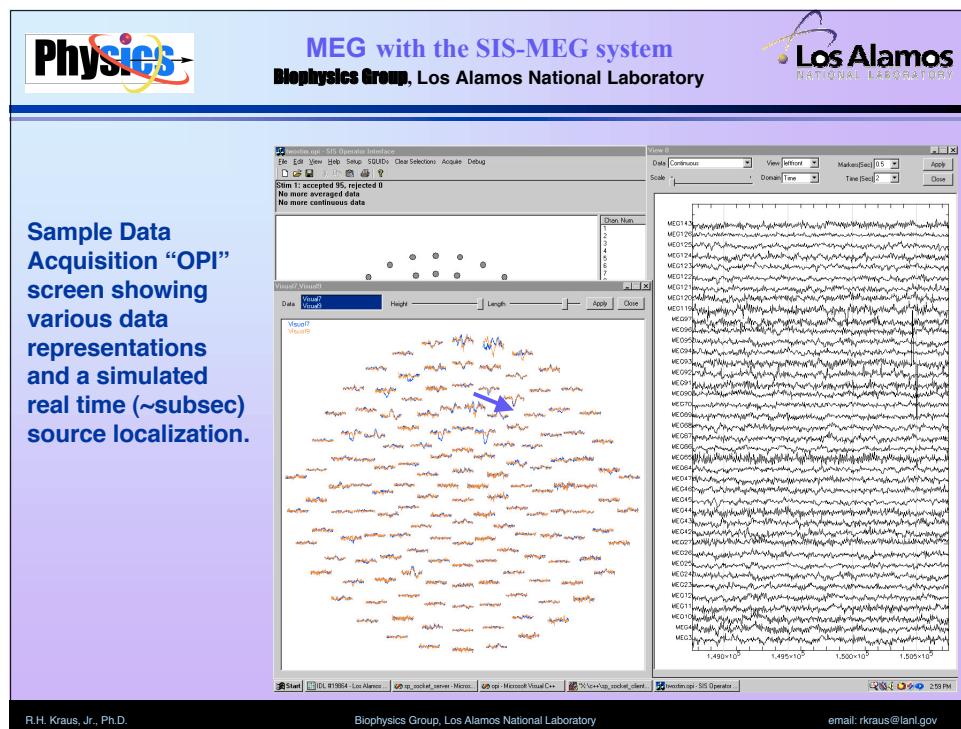
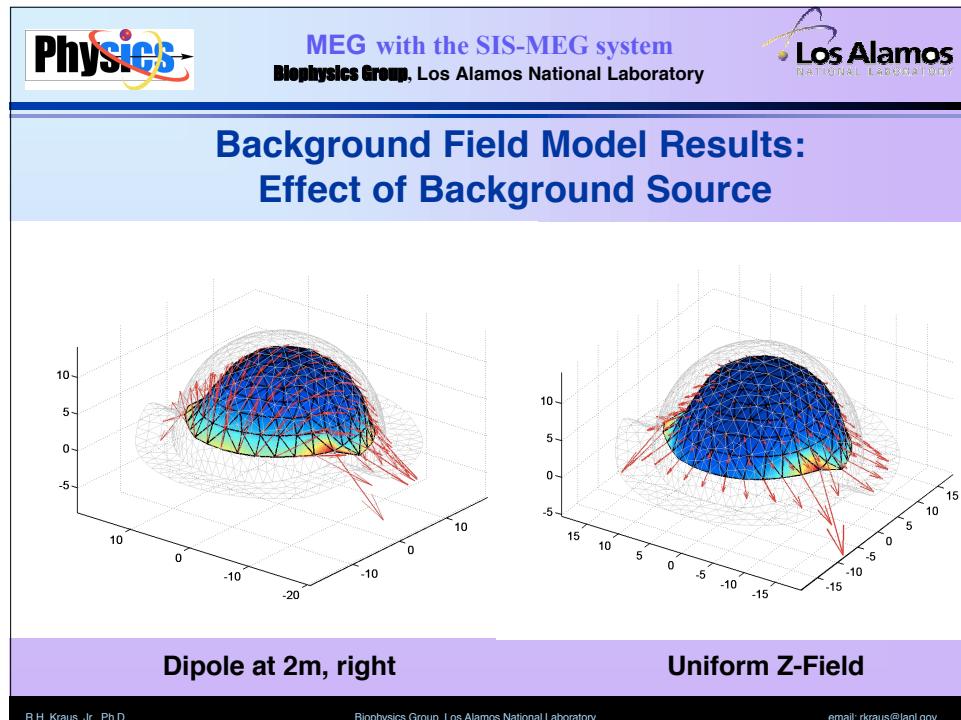
Frequency independent !!
Inherent (low cost)
Strongly source dependent.

Angle above brim (degrees)	Unshielded Cooldown (Shielding Factor)	Shielded Cooldown (Shielding Factor)
10	~150	~100
20	~400	~300
30	~550	~450
40	~950	~850
50	~700	~1100
60	~1350	~1800

Near helmet edges:
Shielding factor observed from ~15 to ~170

Near helmet apex:
Shielding factor observed from ~200 to ~1900

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Conclusions

- Completed FEM description for SIS forward physics (applicable to any superconducting surface)
- Demonstrated excellent agreement between FEM model and experimental results.
- ~2 orders of magnitude frequency-independent shielding demonstrated.
- 0.25mm mean localization accuracy demonstrated for phantom sources.
- Data acquisition system complete/tested
- Real-time source localization in progress (new LDRD)

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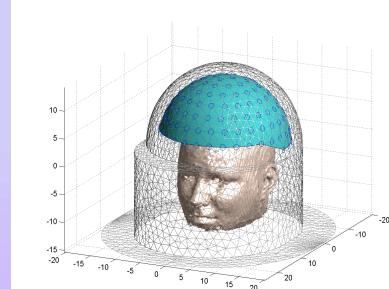
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Near-Term Plans

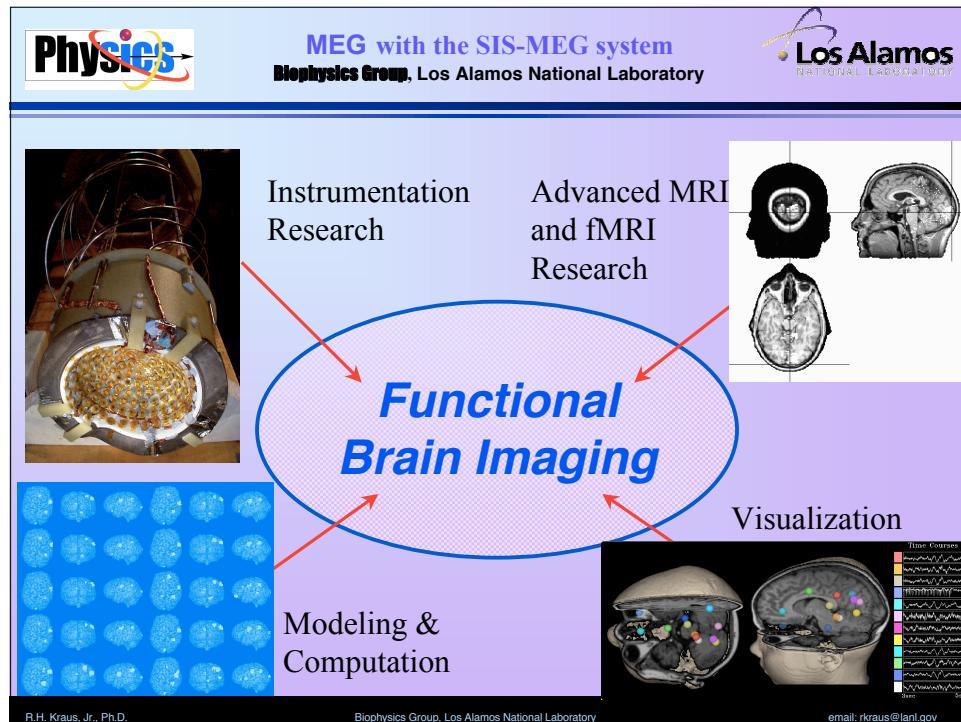
- Locate SIS-MEG system at VA-Albuquerque. Perform efficacy studies with human 'normal.' – NIH, MIND
- Move SIS-MEG system to VAMC-Minn. Perform preliminary measurements on monkeys with implanted electrodes ("gold standard"). NIH Continuation grant to build SIS-MEG optimized for monkeys & incorporating lessons learned.
- Conduct experiments focused on real-time single event analysis with 'feedback.' (Perlmutter, Tang at UNM/VA-Albuq.) - MIND



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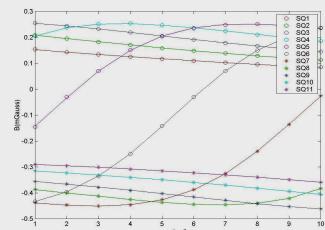
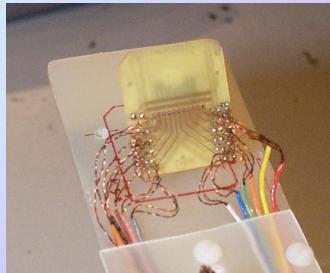
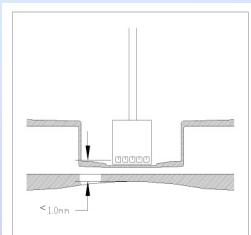
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□-MEG SQUID array & Dewar



High resolution
MEG to observe
activity at the level
of cortical columns

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